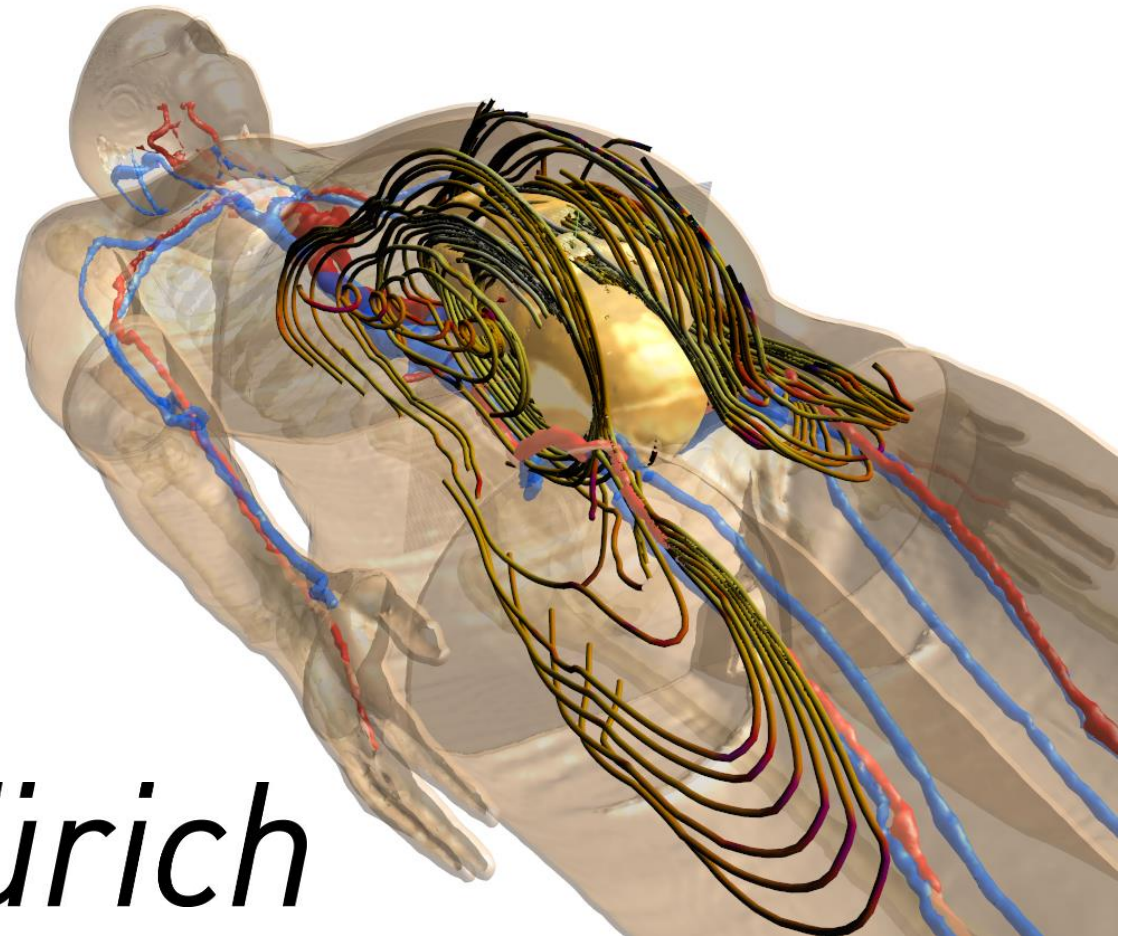


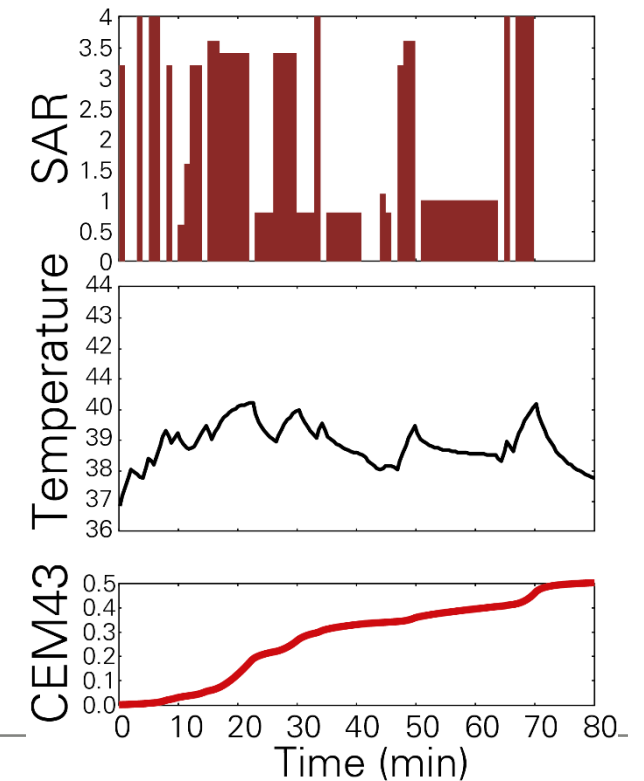
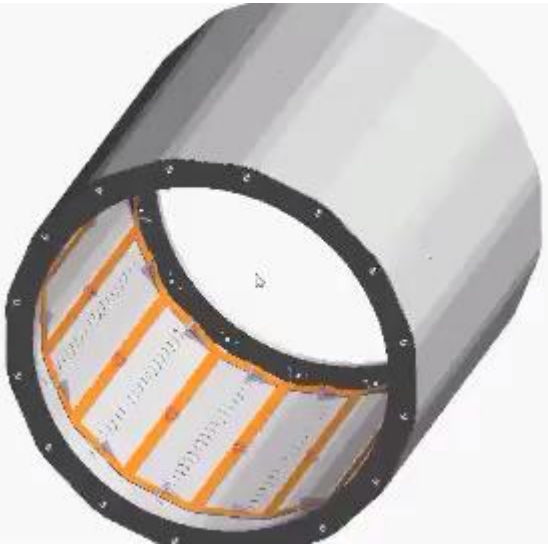
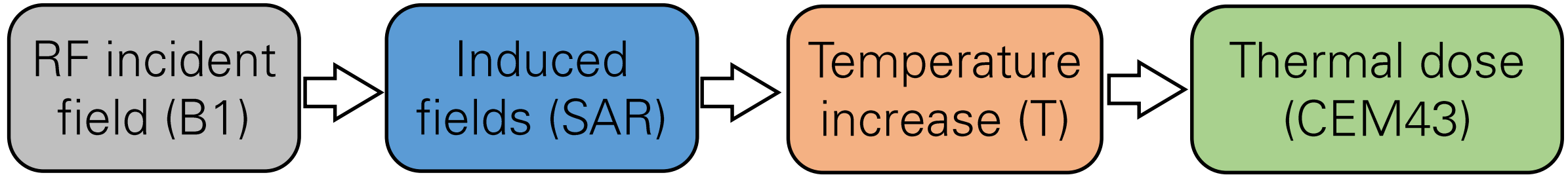
Tissue heating during MR examination as function of RF exposure and local thermoregulation, consequences for the MR safety standard IEC 60601-2-33

Manuel Murbach

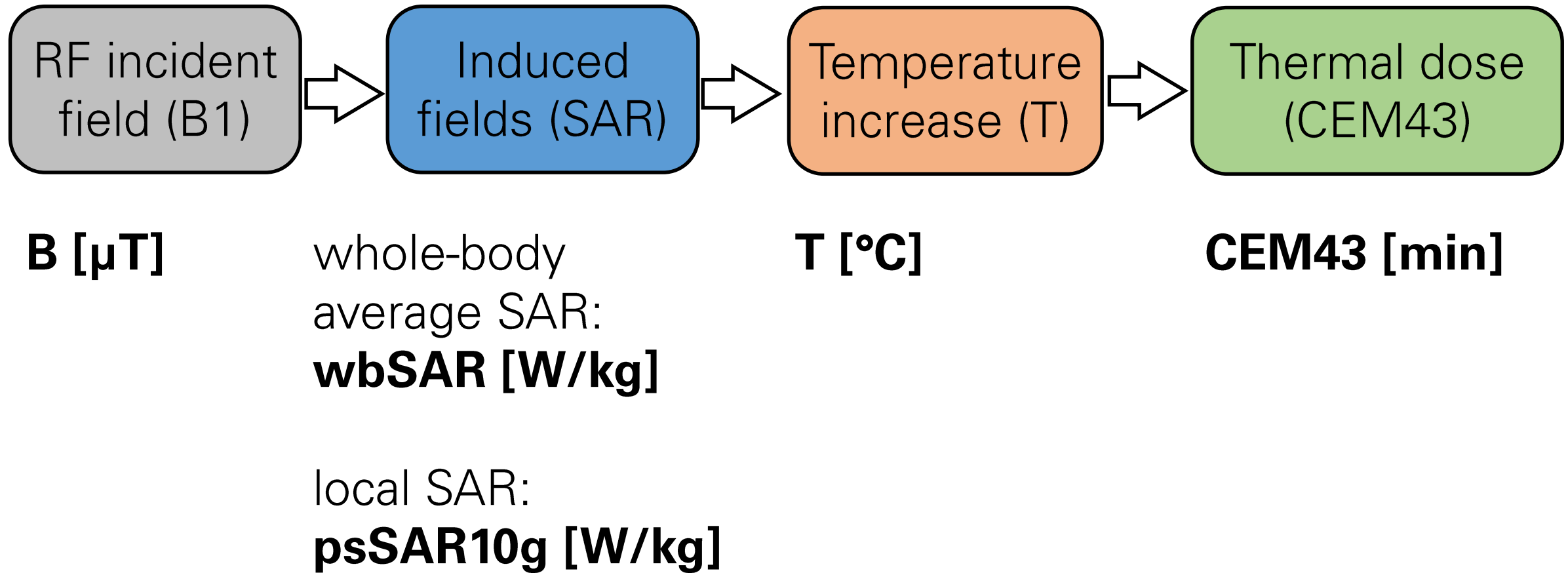
Esra Neufeld, Eugenia Cabot, Earl Zastrow,
Juan Córcoles, Wolfgang Kainz, Niels Kuster



Exposure Chain in MRI



Exposure Chain in MRI



Exposure Safety Management, IEC 60601-2-33

- about 1 billion scans performed within IEC 60601-2-33 limits
- remarkable history of safe use
- **normal** operating mode, **first level controlled** operating mode
- governing limits in temperature (first level: $T < 40^{\circ}\text{C}$)
- ▶ derived limits mainly in **wbSAR** (first level: **wbSAR < 4 W/kg**)
- local SAR is NOT limited for body coils
- ▶ advanced electrothermal simulation modeling shows:
 - ▶ local SAR levels are higher than originally thought
up to $> 80 \text{ W/kg psSAR}_{10\text{g}}$ possible in first level operating mode
 - ▶ local temperature may be higher than envisaged ($> 40^{\circ}\text{C}$)

MRI as a Very Specific RF Exposure Scenario

- exposure configuration well characterized (frequency, incident field distribution)
- patient with respect to the field well defined (posture & landmark position)
- environment very well defined (temperature, clothing, humidity)
- benefit (excellent)
- ▶ specific safety concepts possible

Whole-Body vs. Local Heating

- wbSAR limit is generally providing sufficient protection against **whole-body heating**
 - can be measured reliably via overall dissipated power
 - systemic stress can be assessed, e.g., via subjective well-being of the patient
 - slow changes
- ▶ **local heating, however, may exceed assumed limits**
 - cannot be measured directly, simulation models are necessary
 - local temperatures may not be adequately perceived (e.g., limited heat sensation in muscle tissue)
 - multitransmit / pTx makes predictions more complex
 - ▶ **environment (air temperature, ventilation, sweating) does NOT affect local temperature hotspots inside the body**

Study Overview

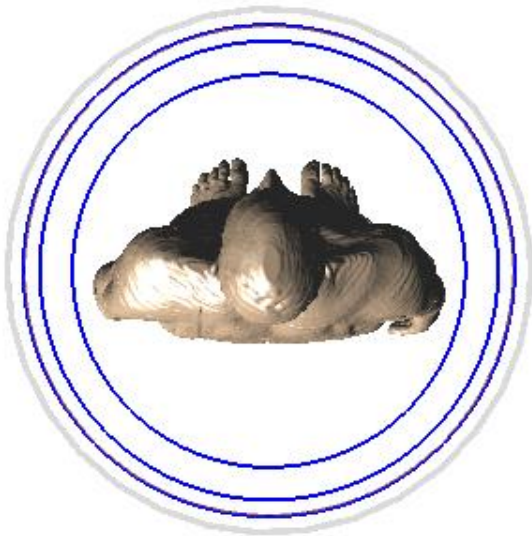
- non-implant RF heating
 - 2011: local SAR enhancements [Murbach et al., 2011]
 - 2011: multitransmit SAR [Neufeld et al., 2011]
 - 2014: correlation with anatomy [Murbach et al., 2014b]
 - 2014: thermal damage evaluations [Murbach et al., 2014a]
 - 2015: CEM43 safety supervision concept [Neufeld, et al, 2015]
 - 2015: RF-Shimming with pregnant women [Murbach 2015, in preparation], [Murbach et al., 2014c]
 - 2015: RF-Shimming with pregnant women [Murbach 2015, in preparation]
 - 2015: pTx for pregnant women [Murbach 2015, in preparation]
- implant RF heating
 - 2009: MRI implant heating [Neufeld et al., 2009]
 - 2011: implant safety [Kyriakou et al., 2011]
 - 2012: RF heating of DBS [Cabot et al., 2012]
 - 2014: validation system of Tier 3 method [Zastrow et al., 2014]
 - 2015: implant RF-heating mitigation [Zastrow 2015, in preparation]
- other
 - JWG: [ISO/TS 10974, 2012]
 - 2013: CEM43 Tissue Damage Thresholds for MR [van Rhoon et al., 2013]

Incident Field

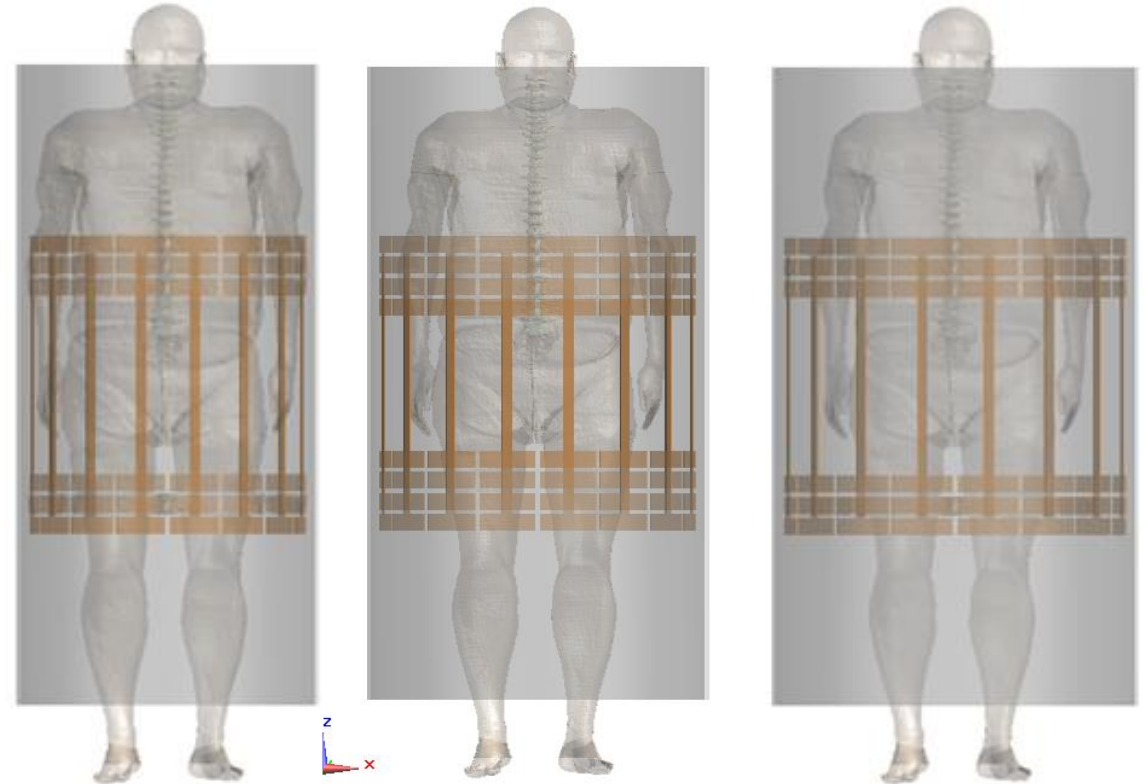
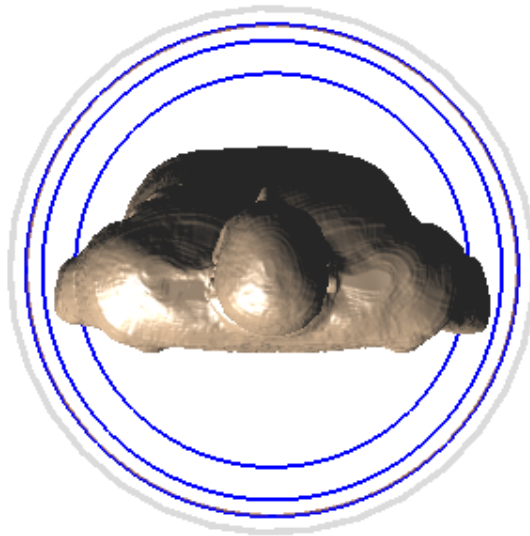
▶ body coil model ("antenna")

- excitation scheme (CP, RF shimming)
- birdcage dimensions:

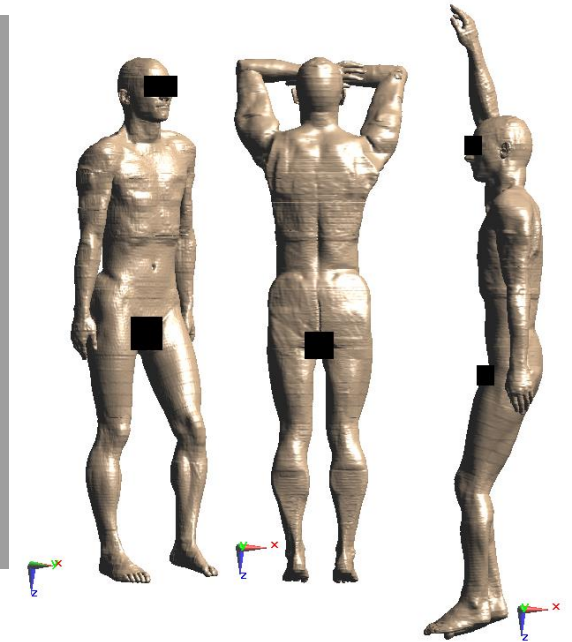
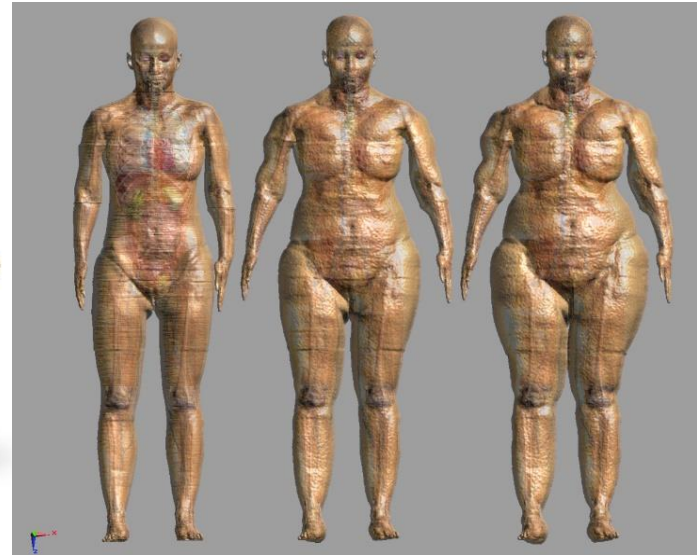
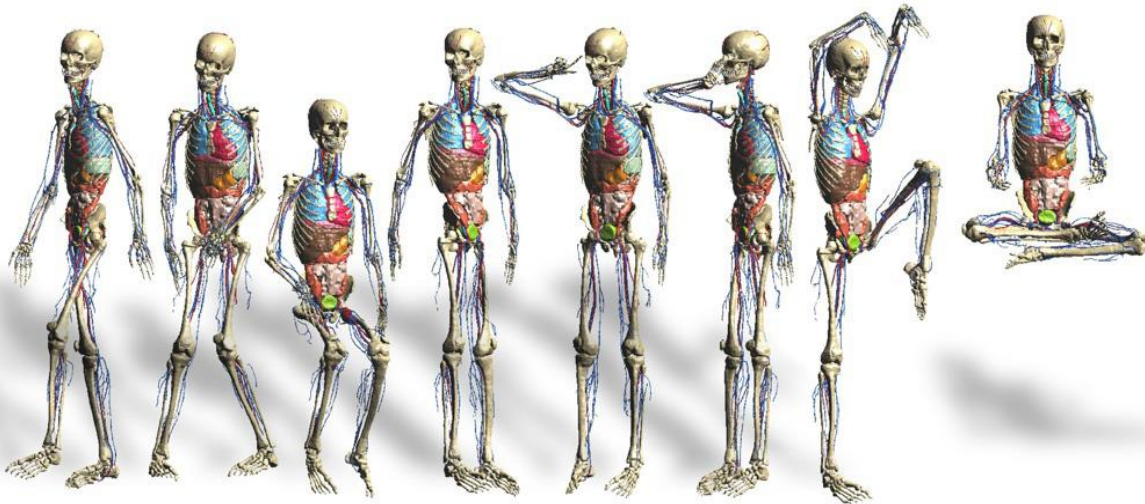
Duke



Fats

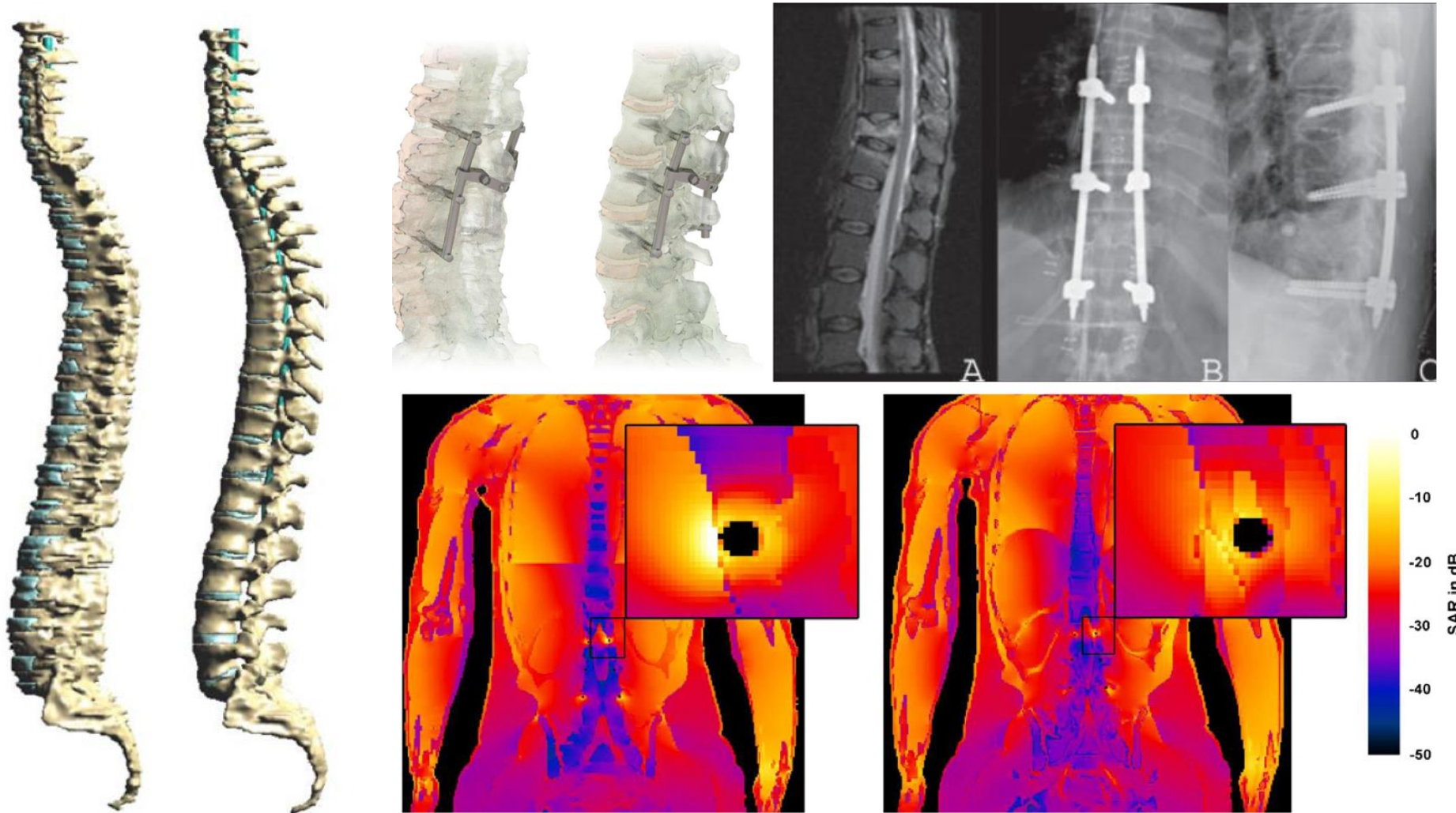


Anatomical Models: Posing / Morphing



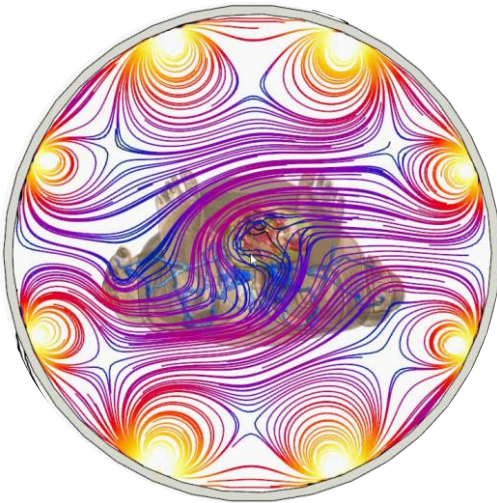
- anatomical human models, e.g., Virtual Population
- posing: volume preserving posture changes
- physics-based morphing to enhance range of coverage
- ▶ increased population/situation coverage

ViP 3.0 - Approaching Clinical Realism

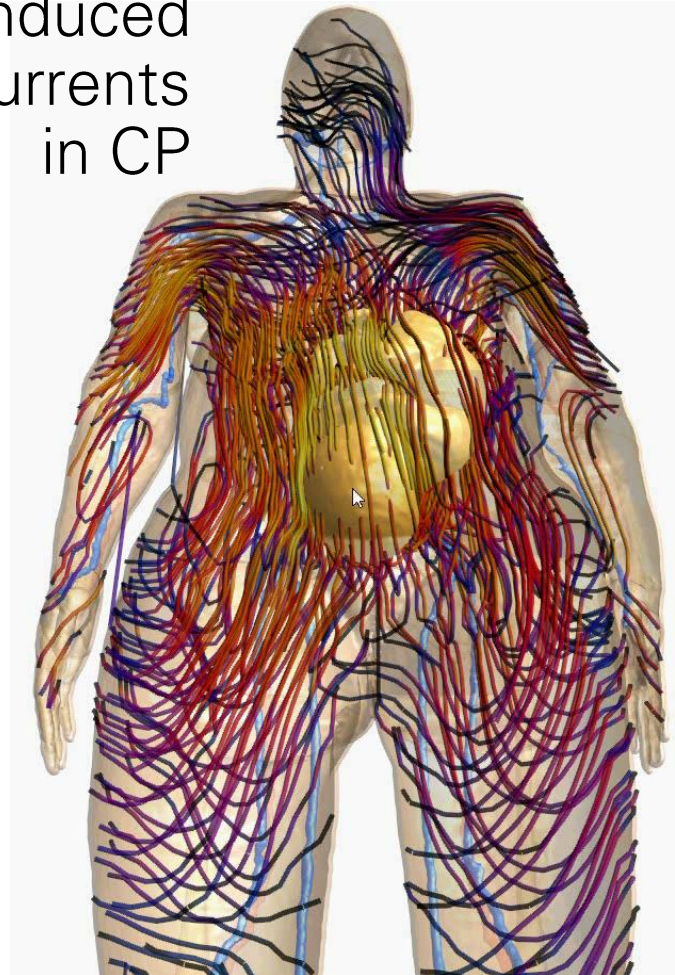


Exposure Pathway through Induced Eddy Currents

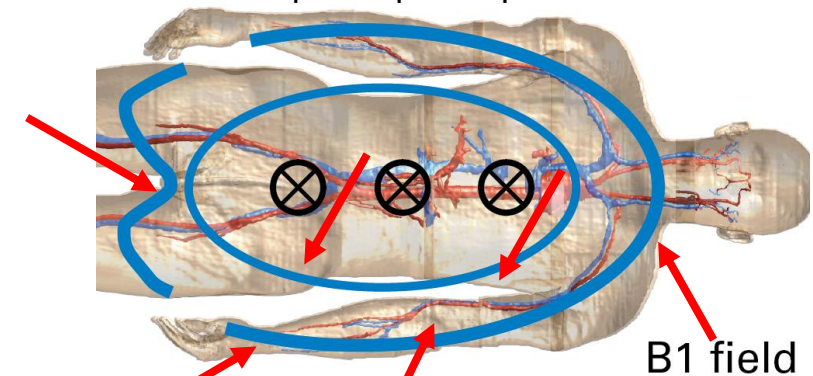
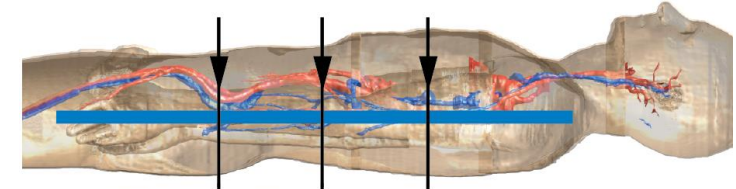
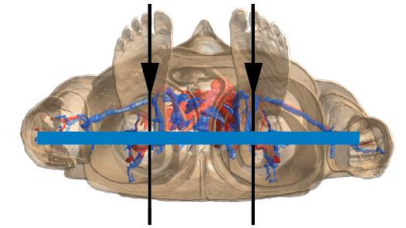
B1-Field in CP



induced eddy-currents in CP



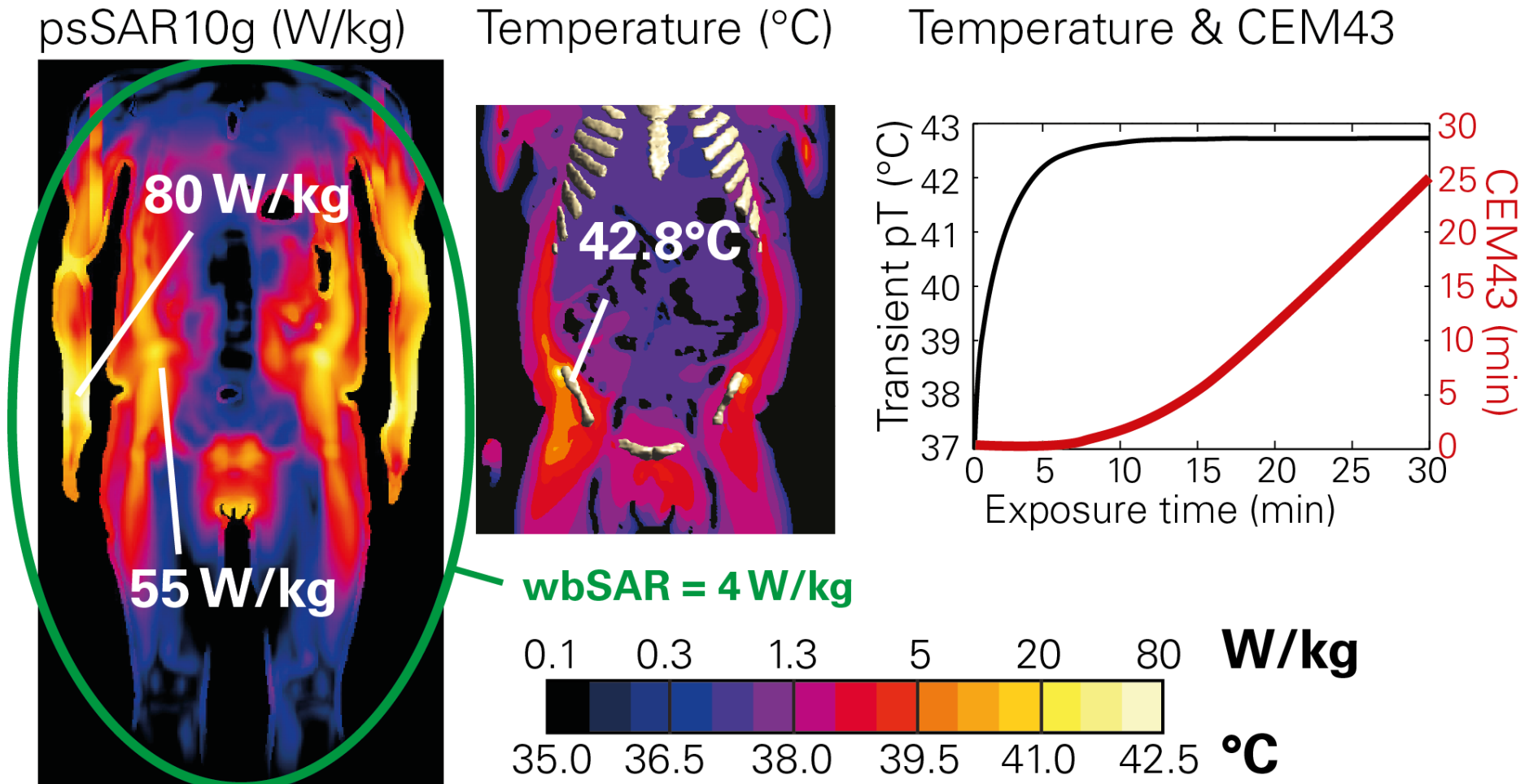
vertical B1 polarization



typical «hotspot» locations

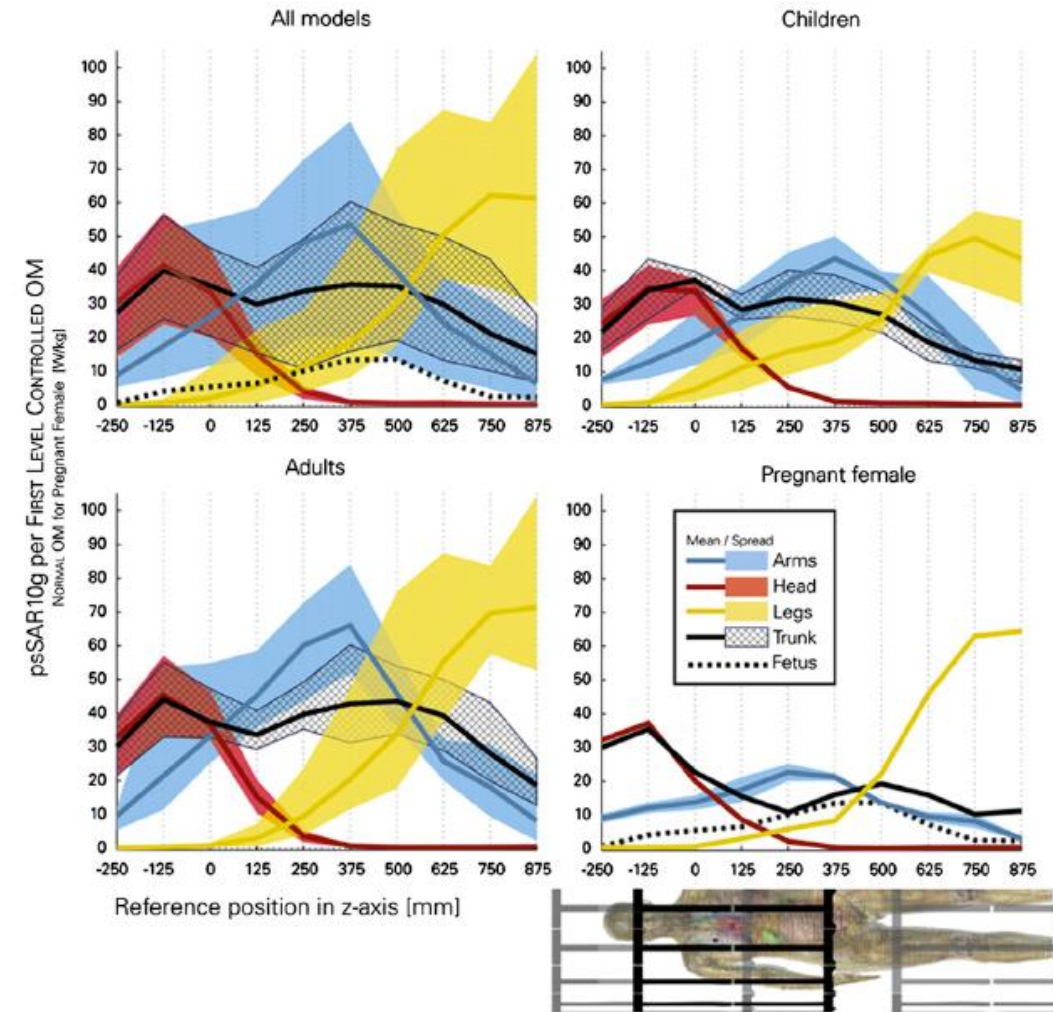
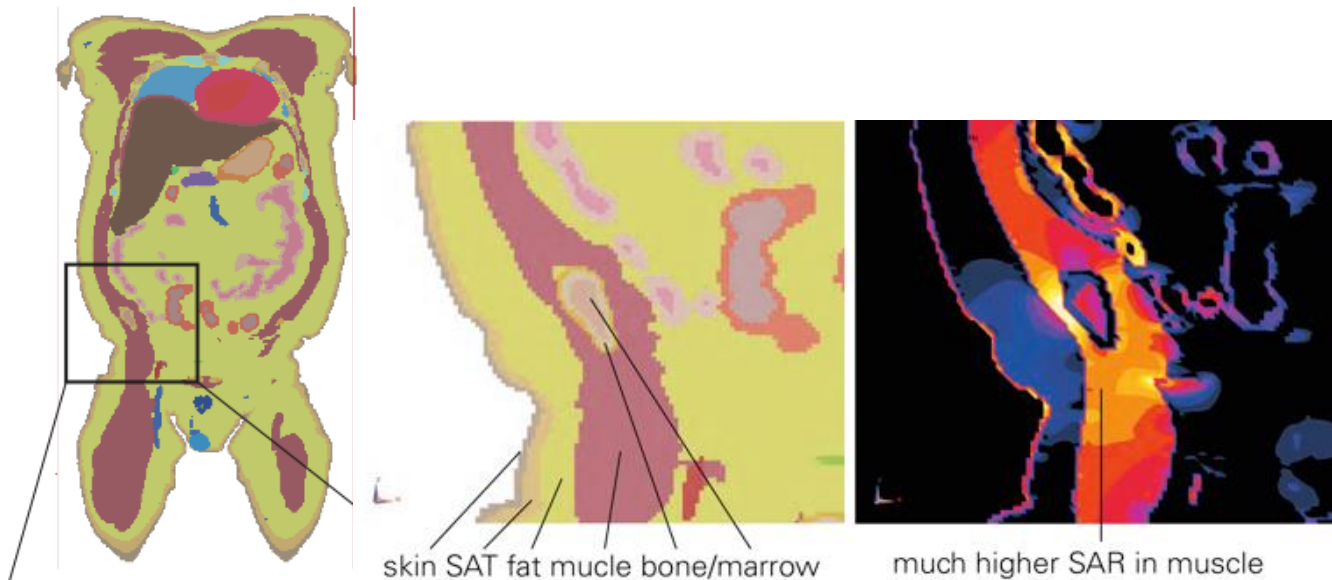
Example High-SAR Scan Scenario

- Fats (obese model)
- pelvis imaging position
- 1.5T CP
- ▶ maximum allowance (wbSAR = 4 W/kg)



2011: Local SAR Enhancements (1.5T)

- ▶ local SAR (psSAR10g) can reach > 80 W/kg (in First Level OM)

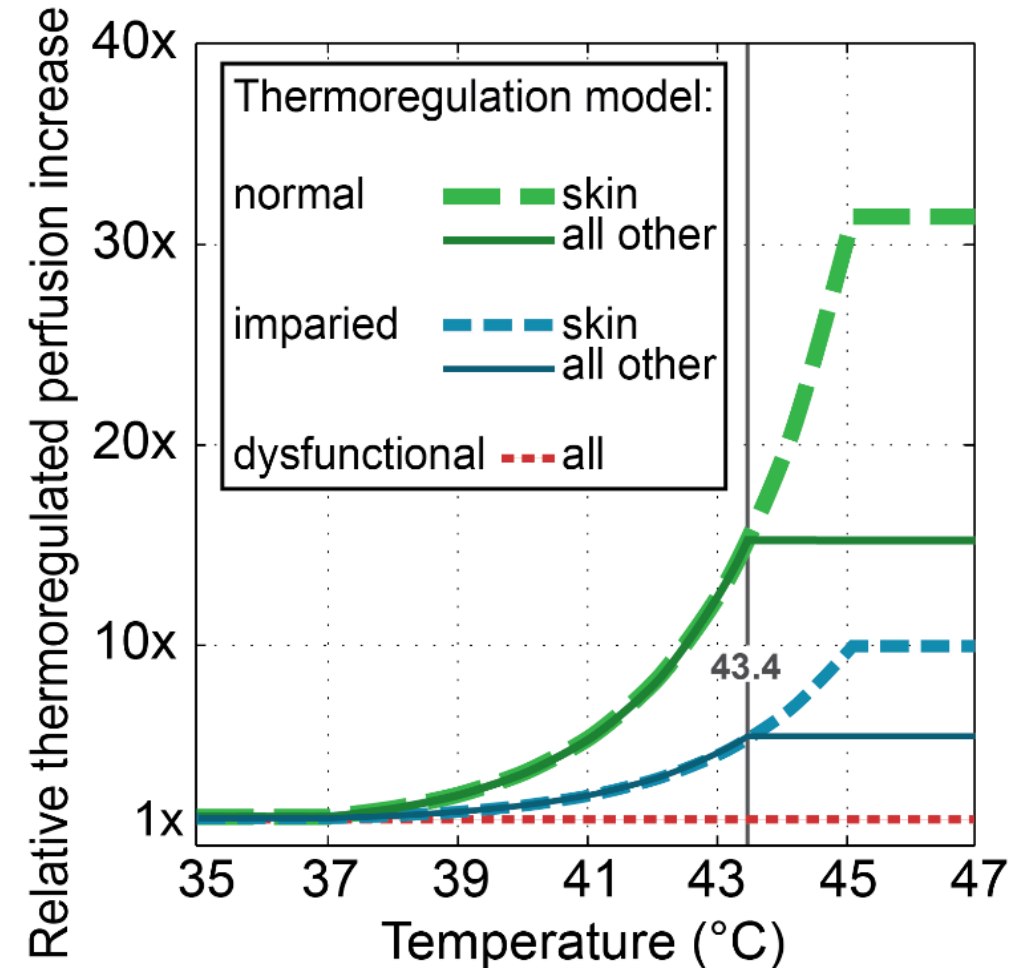


Local Thermoregulation Model

- ▶ local thermoregulation is the most important parameter for local temperature increases [Laakso & Hirata 2011] for MR exposures (> 20 W/kg)
- thermally induced blood-flow increase of factor > 10
- the ability to up-regulate the local blood-flow has often been underestimated

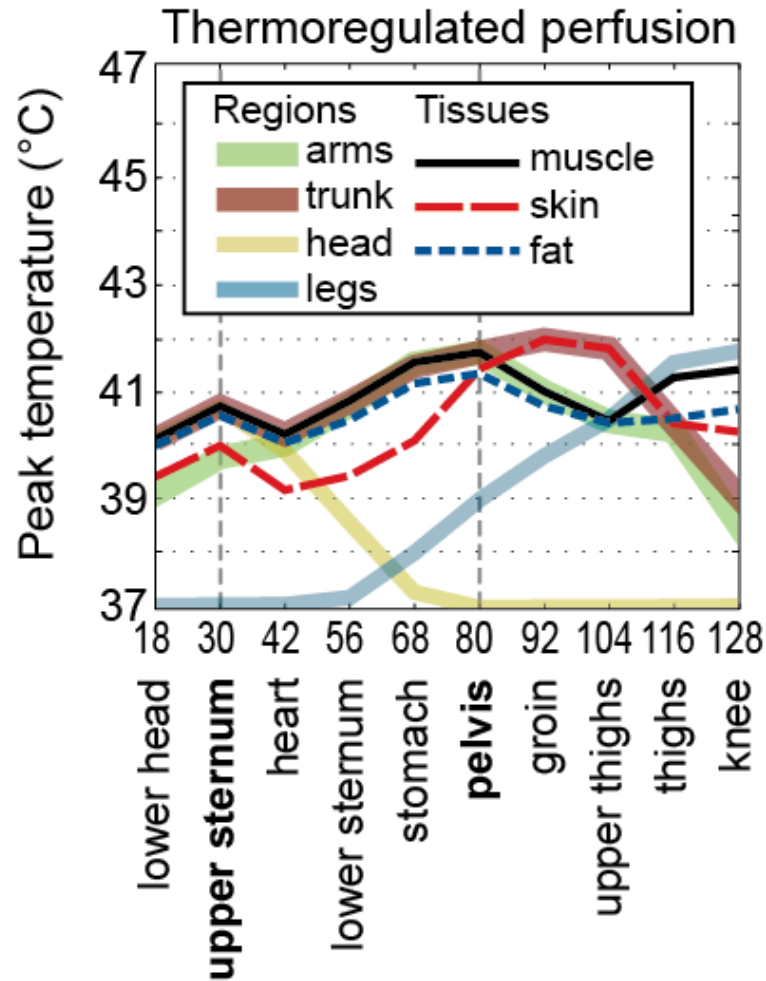
Local Thermoregulation Models

- we suggest the following definitions
 - ▶ normal thermoregulation: factor 32 (skin) and 16 (other) increase
 - ▶ impaired thermoregulation: 70% reduction in perfusion change
- impaired thermoregulation for conservative estimations
- thermal hyperaemia is impaired in: diabetes, age, smokers, renal failure, cardiovascular disease. (range: 21% - 61%)

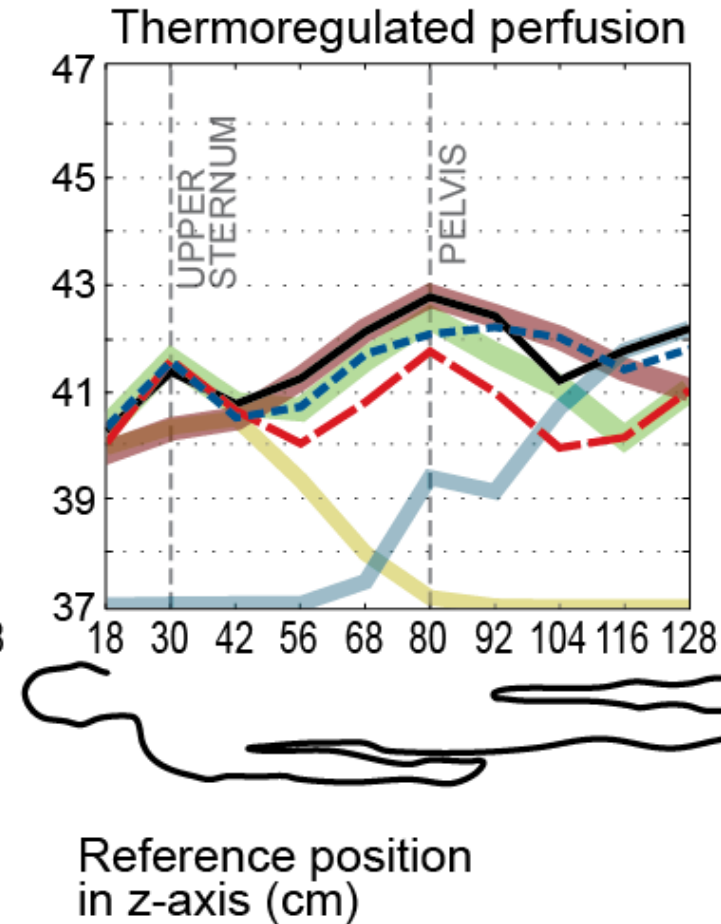


Local Temperature Evaluations (1.5T)

Duke

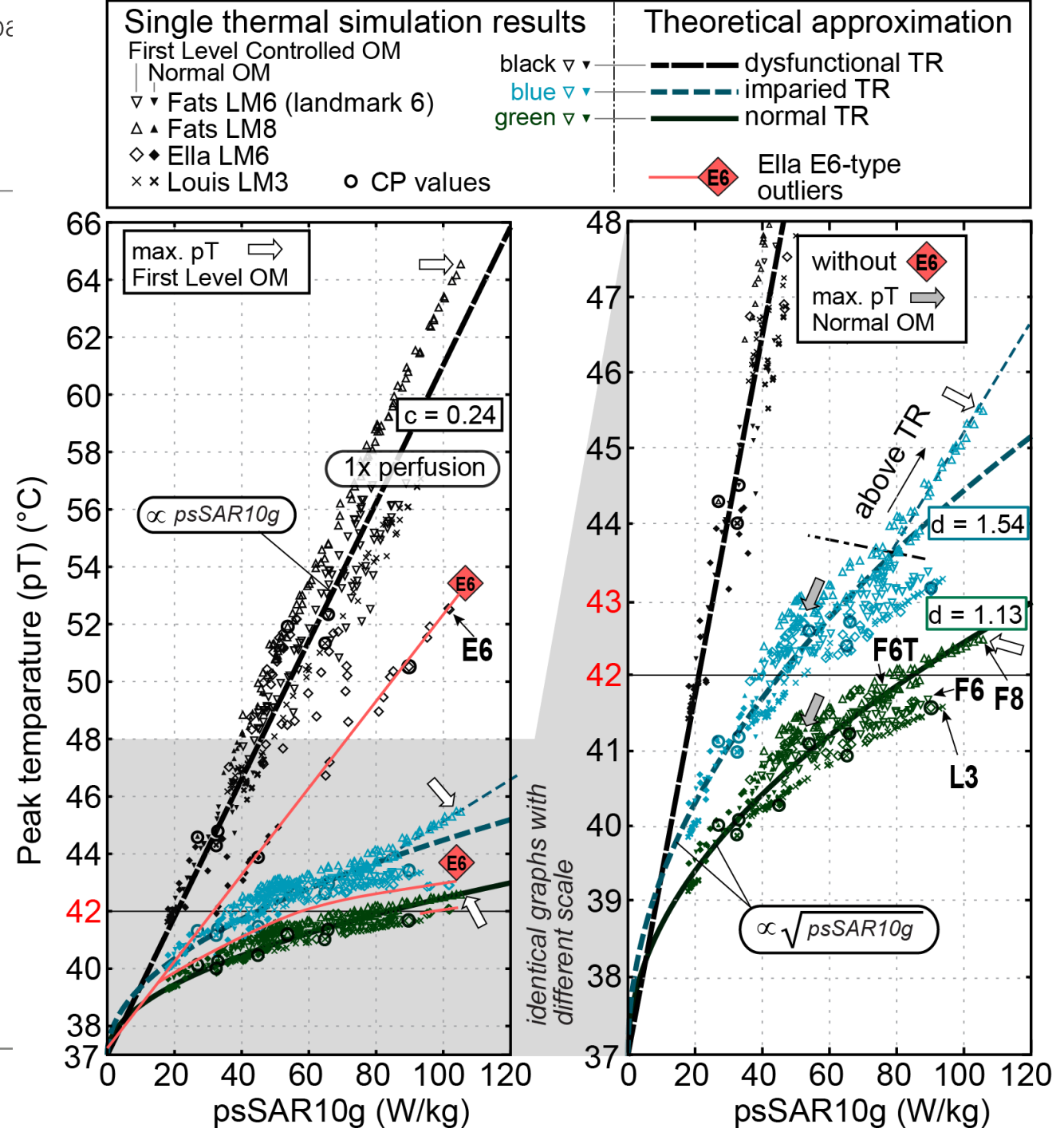


Fats



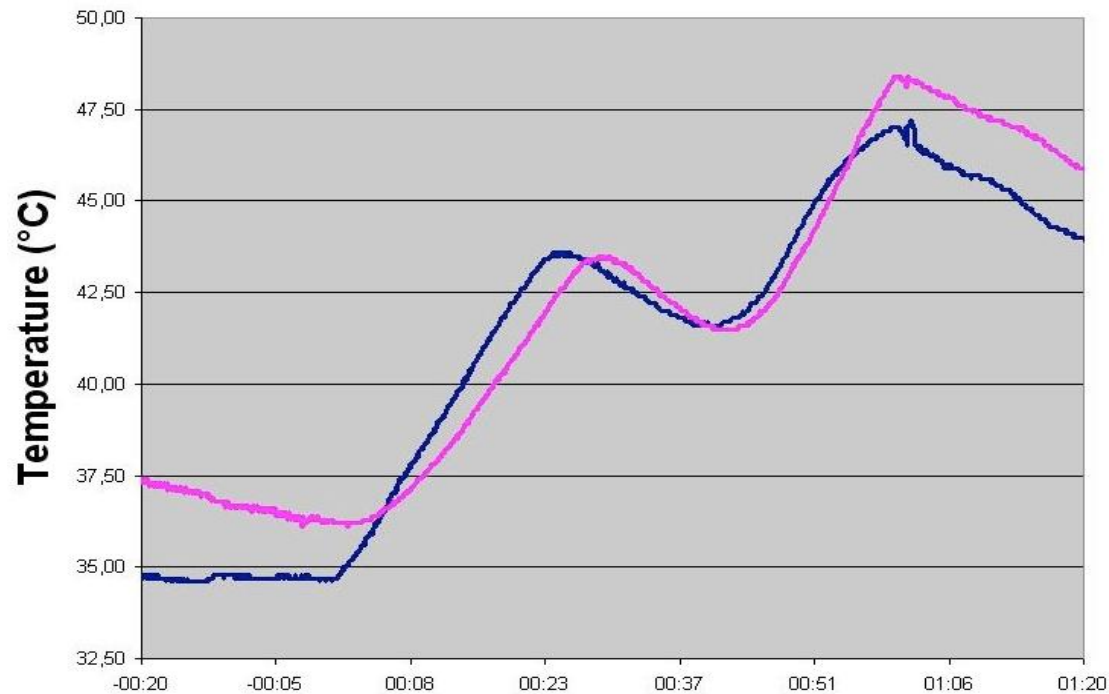
Local Temperature (3T)

- data from 3T 2-port shimming
- 4 worst-case scenarios with Fats, Ella, and Louis, considering various RF shimming excitations
- good correlation with theoretical approximations published in [Neufeld 2015]

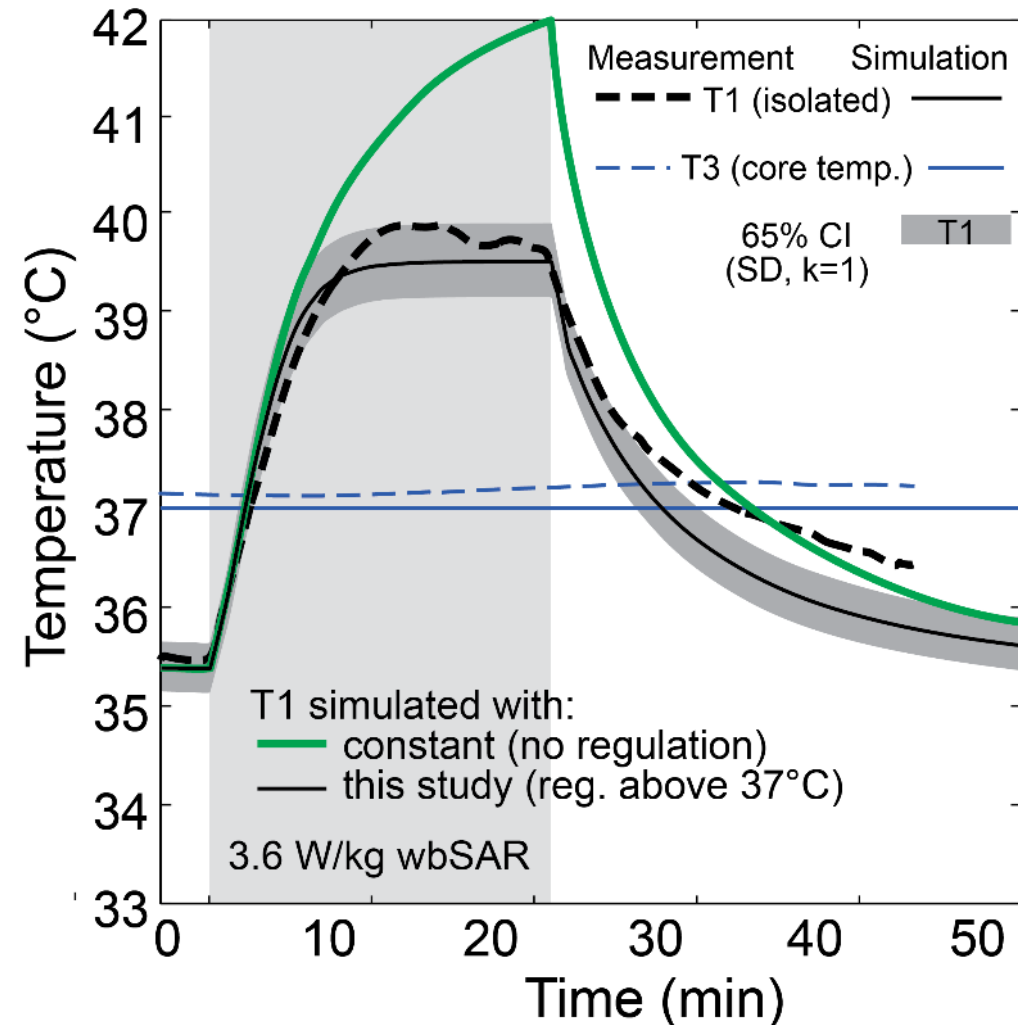
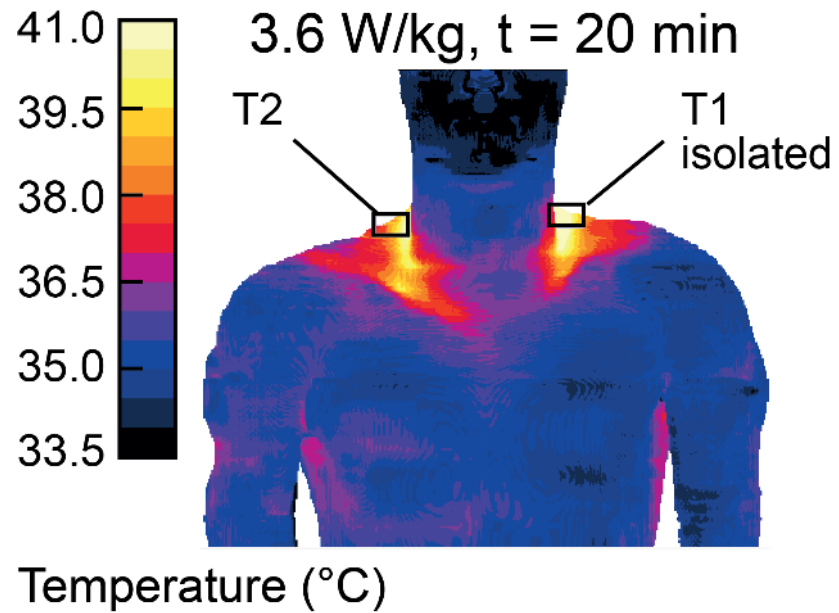


Reality Check: In Vivo (swine)

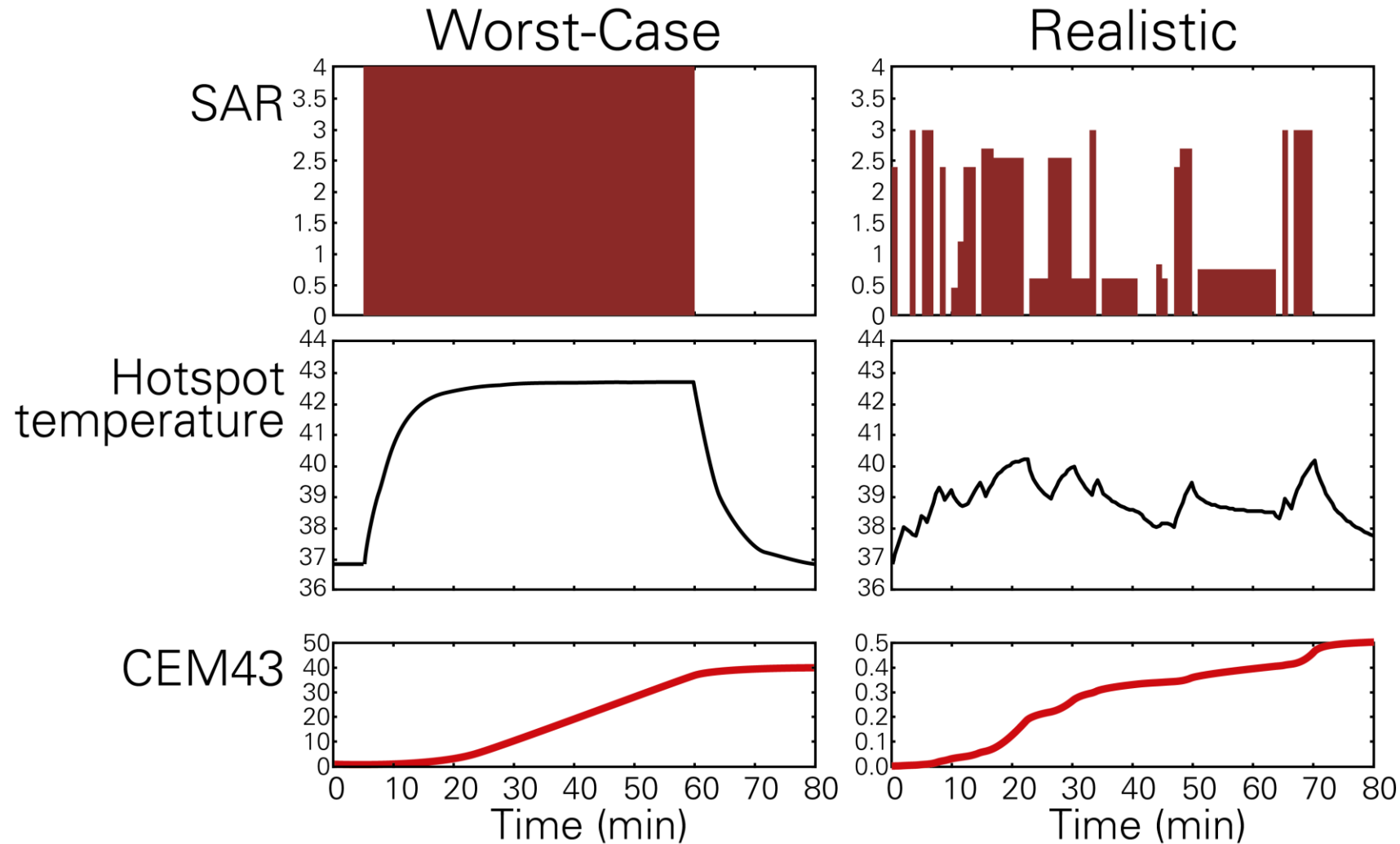
- data from MRI+ partners Charité/Siemens
 - ▶ Evaluation of #24, $wbSAR=4$ W/kg, $t_{expo}=60$ min
 - ▶ NOTE: this exposure level is allowed for human exposure



Local Temperature Validation in Human



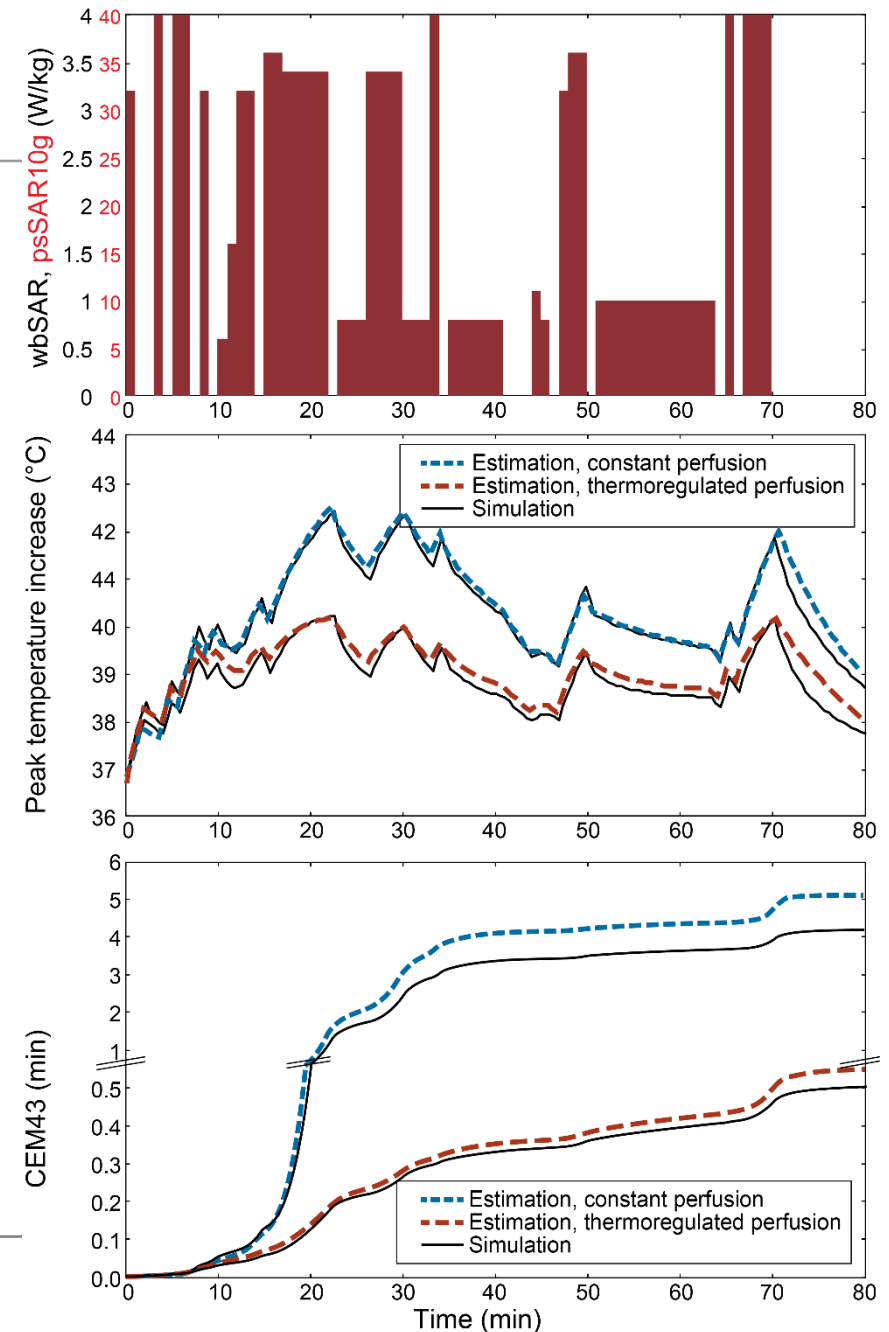
Thermal Dose Accumulation



$$\text{CEM43} = \int_0^{t_{\text{duration}}} R^{T(t)-43} dt$$

Rapid Method for Dose Estimation

- Neufeld E, Fuetterer M, Murbach M, Kuster N. Rapid method for thermal dose-based safety supervision during MR scans. Bioelectromagnetics 2015 10.1002/bem.21919 (early view)
- exponential approximations of temperature, based on SAR
- peak temperature and time constant derived from simulations
- model can include local thermoregulation
- good agreement between model prediction and full simulation results



Conclusions

- enforcement of ICNIRP localized SAR limits would be too conservative
- strict enforcement of the current temperature limits (39°/40°) may be very restrictive and overly conservative regarding the history of safe use
- ▶ risk-benefit analysis and the well controlled environment (exposure/environment) justify a more progressive safety concept
- ▶ governing limitations should be based on thermal dose (CEM43) rather than temperature or local SAR

Consequences for MR Safety Standard IEC 60601-2-33

- thermal dose considerations are more appropriate than current limits
- thermal dose considerations may provide improved rationales for current/future exposure safety management
- proposed multi-tier approach:
 - **TIER1: Conservative SAR considerations**
 - **TIER2: SAR-based conservative thermal dose (CEM43) estimation**
 - **TIER3: Modeling of the thermal response of the patient**
considerable progress in recent years. However, workflow for patient-specific estimates is not yet ready
- find agreement on safe thermal dose limits (e.g. CEM43 = 2min)

Open Questions

- reset time of CEM43
 - when can we start again with $CEM43=0$, after X hours?
 - ▶ 3 hours [Yarmolenko], safety margin?
- large low- or non-perfused regions (pathological, temporary constrictions)
- highly localized hotspots, e.g. RF loops
- conservativeness, how and where apply appropriate safety margins
- patients in anesthesia (no patient feedback)
- medication potentially compromising thermoregulation
- thermal hysteresis, thermal memories, resilience

Thank You

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